



Magnetic rotational spectroscopy : a novel active microrheology technique for colloids and gels

Jean-François Berret



Rheology

Rheometer



Shearing device



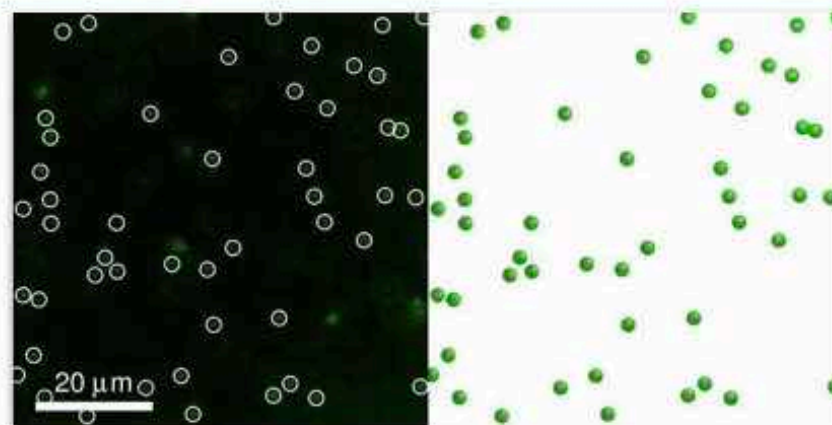
Micro-rheology

Microscope



Micron-sized probes

web.mit.edu/savin/Public/





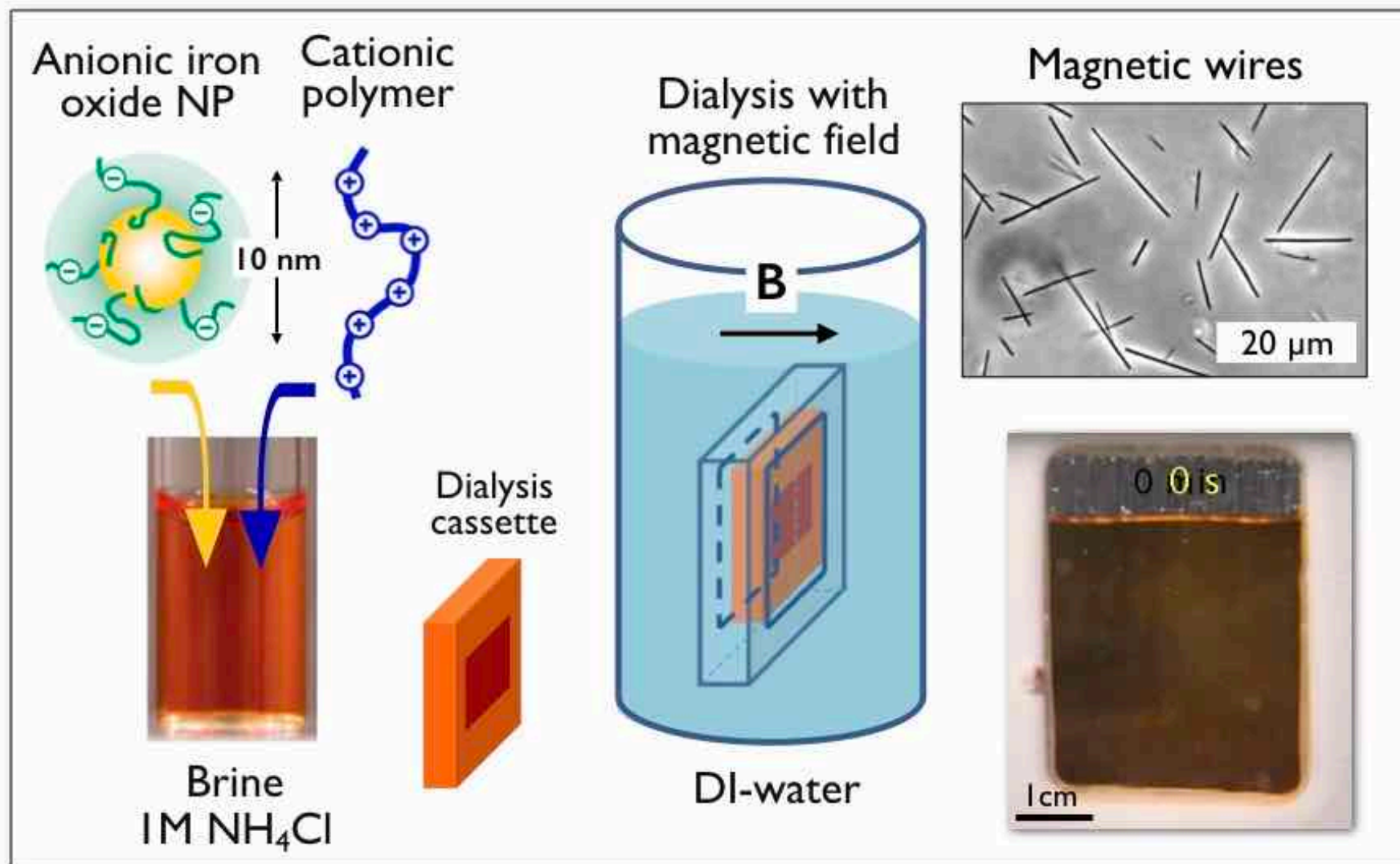
Matière et Systèmes Complexes

I - The tools

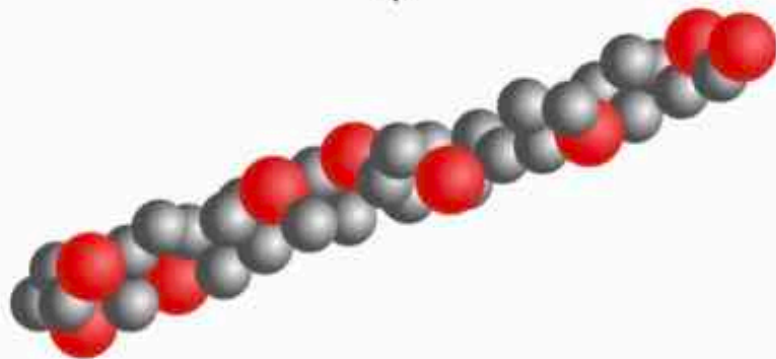
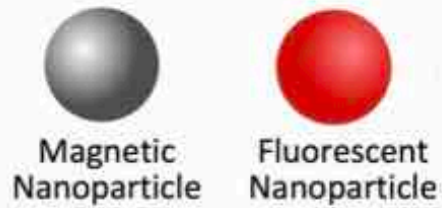
II - Rheological models and validation

III - Applications to lung fluids

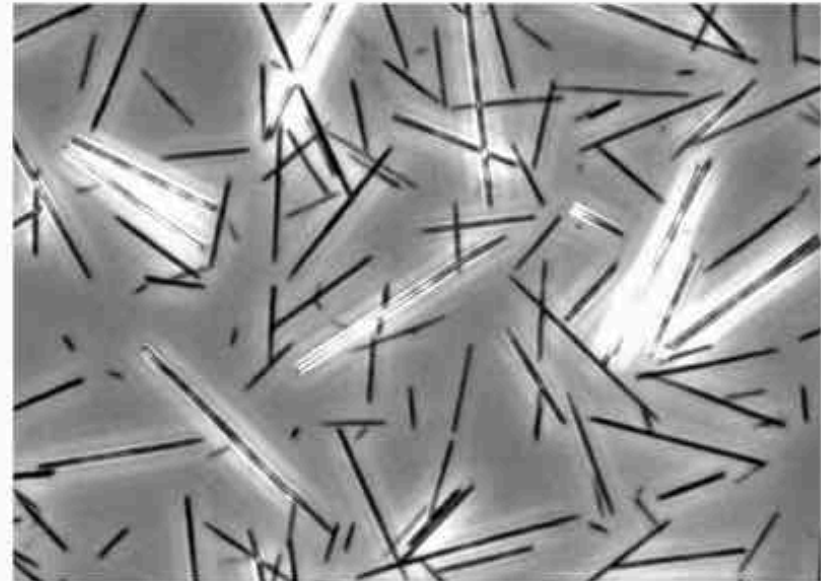
Probe fabrication



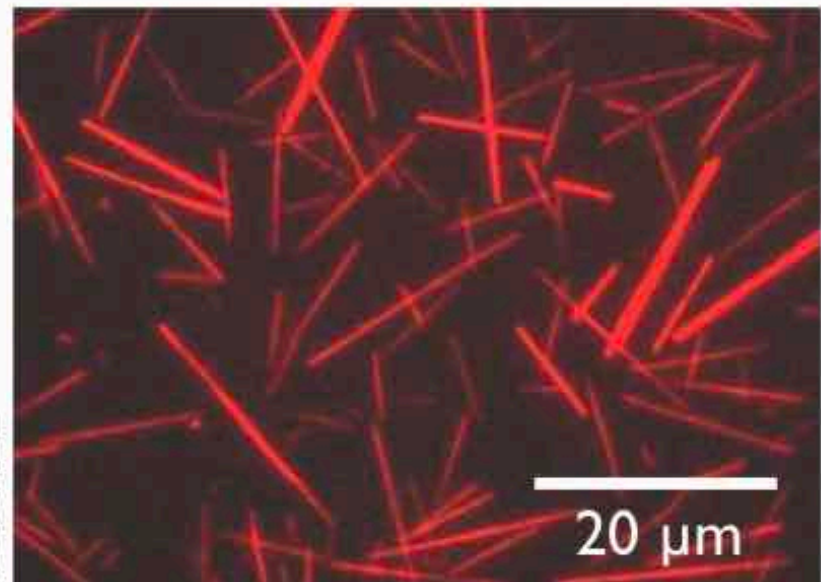
Mixing magnetic nanoparticles and fluorescent quantum dots prior to dialysis



Phase contrast

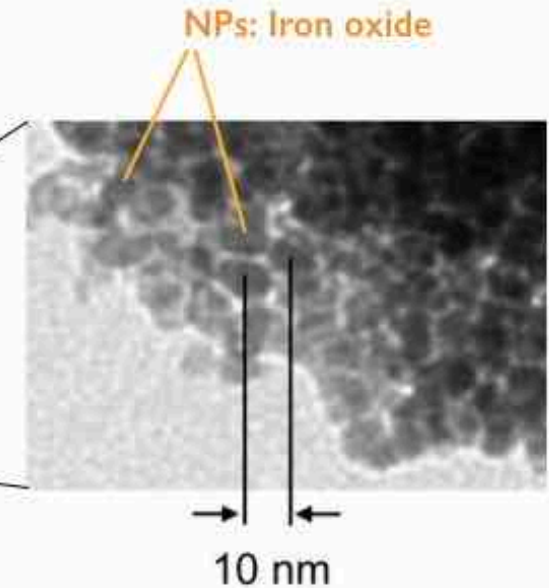
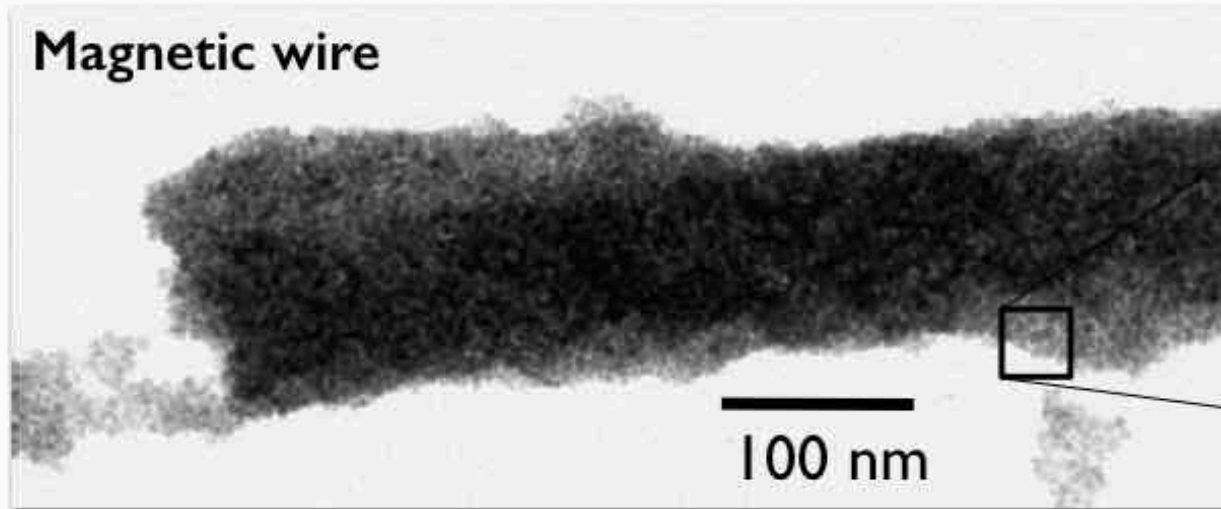


Emission fluorescence
at 600 nm



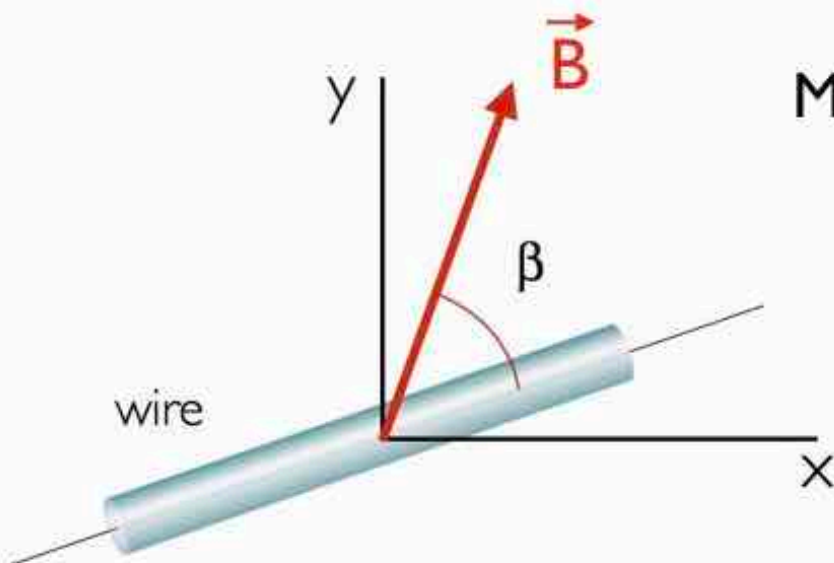
TEM

Magnetic wire



Volume fraction of particles
30 vol. %

Magnetic torque



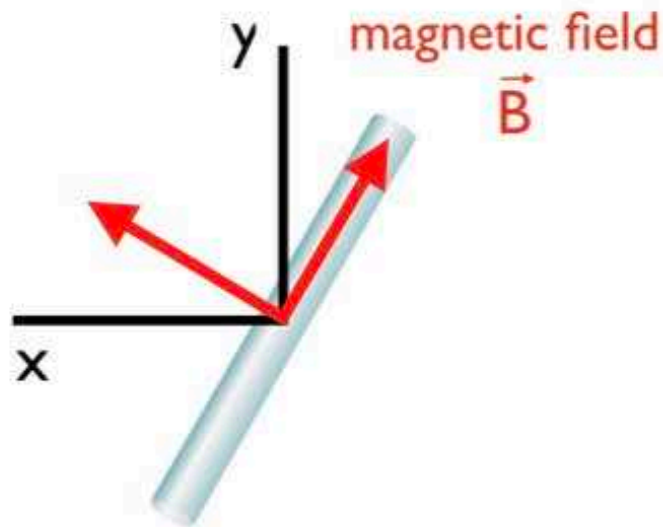
$$\Gamma_{Mag} = \frac{1}{2\mu_0} V \Delta\chi B^2 \sin(2\beta)$$

Wire volume

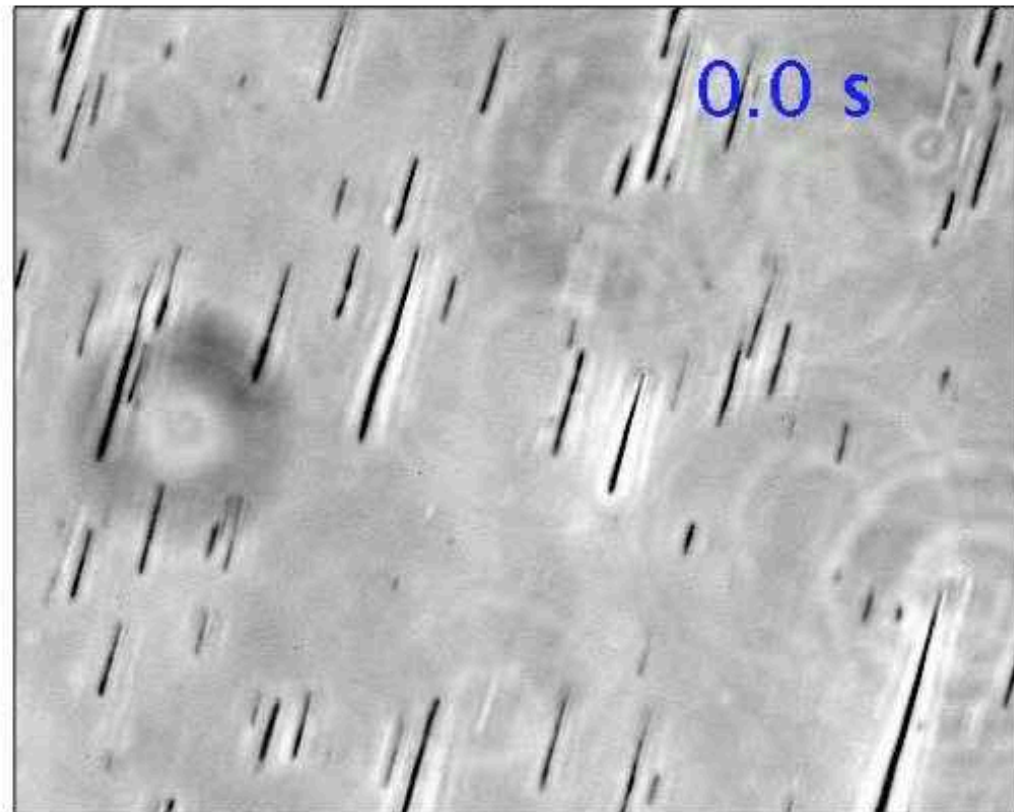
Susceptibility
anisotropy

Magnetic field

90°-flip of the magnetic field



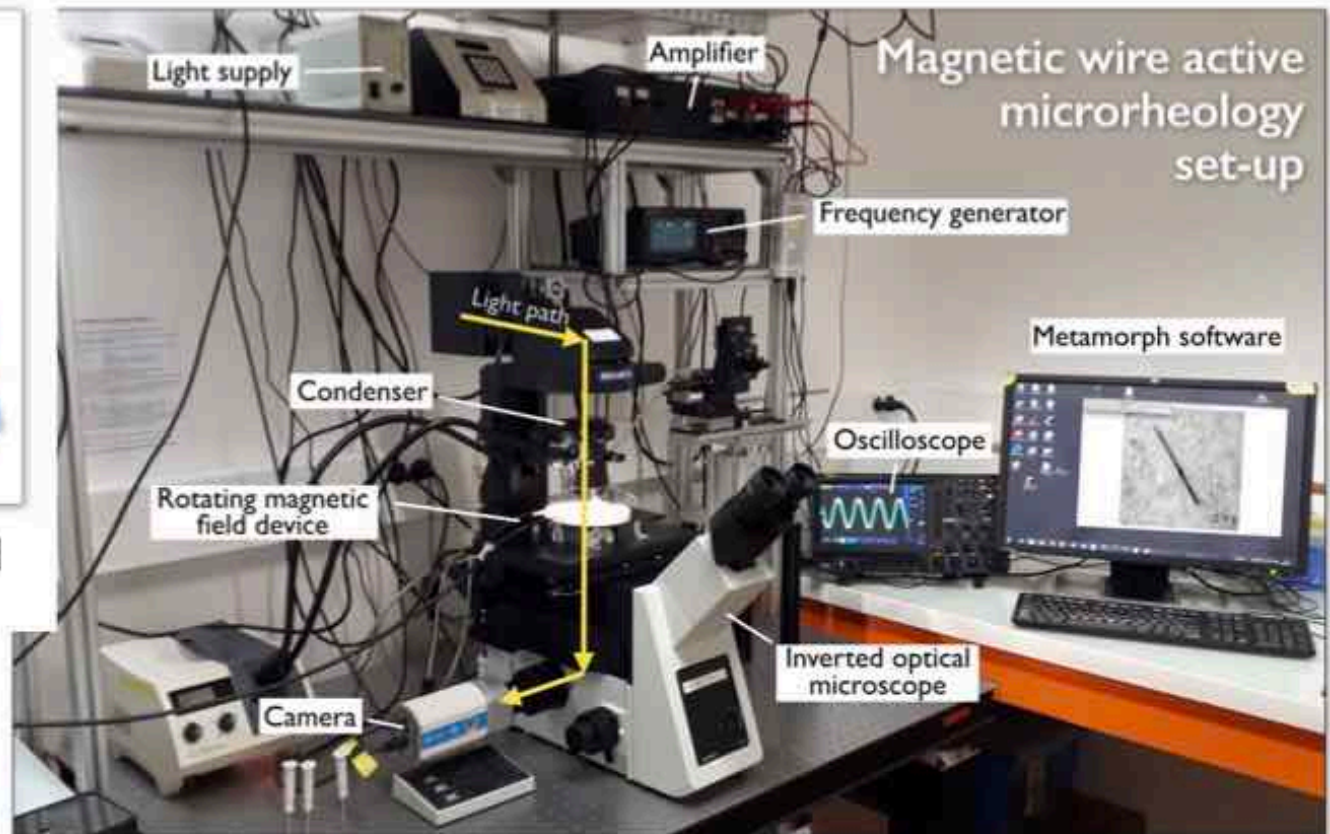
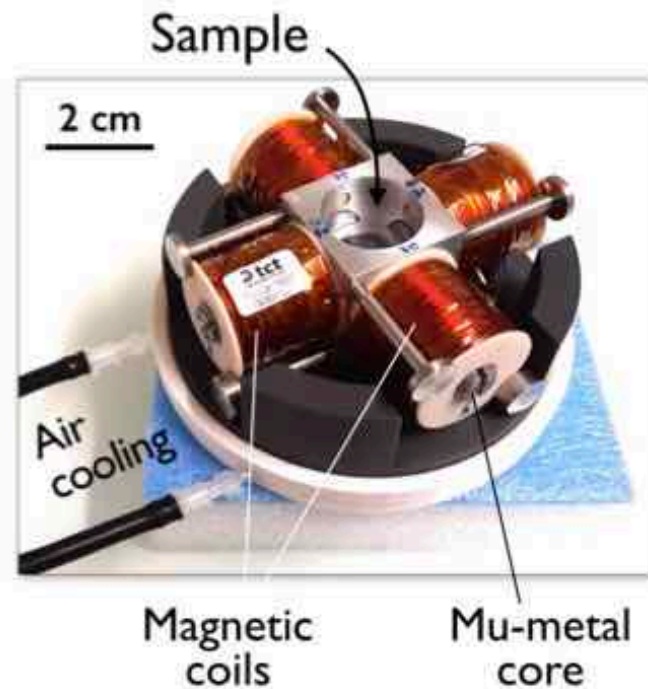
20 μm

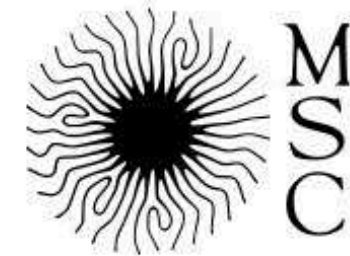


- The wires are superparamagnetic
- Their response to a field depends on the length and diameter

Magnetic Rotational Spectroscopy*

In MRS, micron-sized wires are submitted to a rotational magnetic field ($1 - 50 \text{ mT}$) as a function of the frequency ($10^{-4} - 100 \text{ Hz}$)





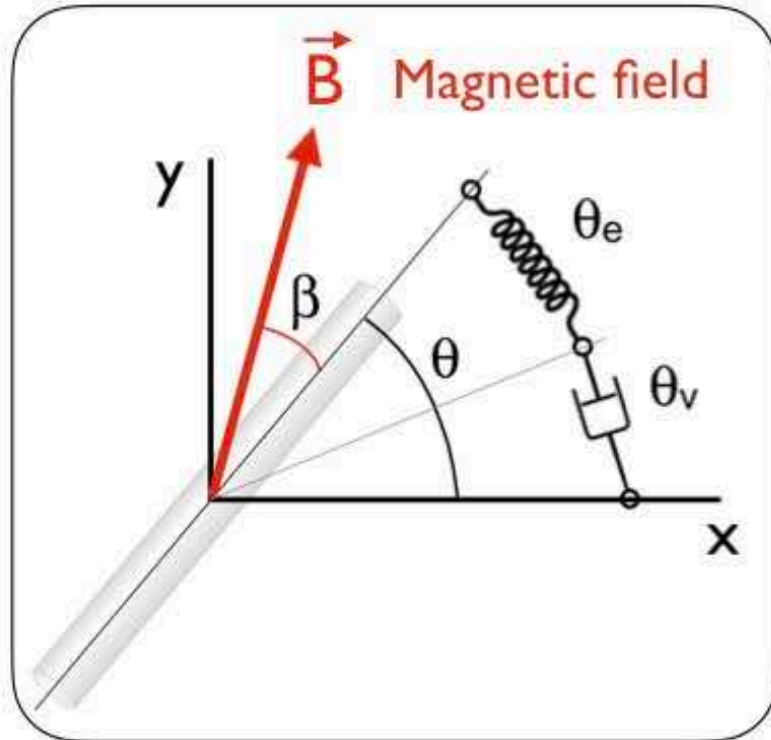
Matière et Systèmes Complexes

I - The tools

II - Rheological models and validation

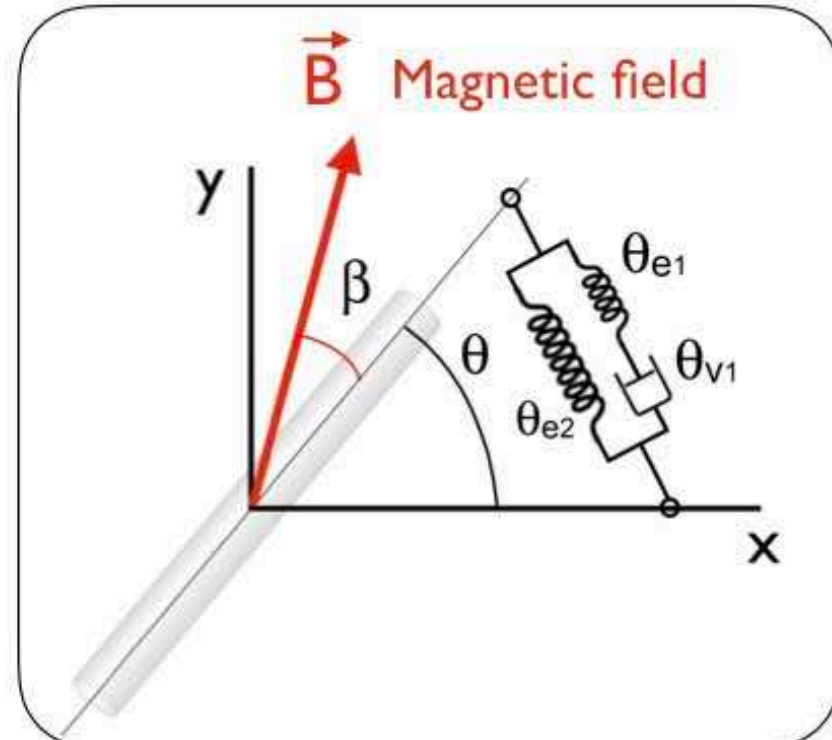
III - Applications to lung fluids

Maxwell model



→ Viscoelastic liquids

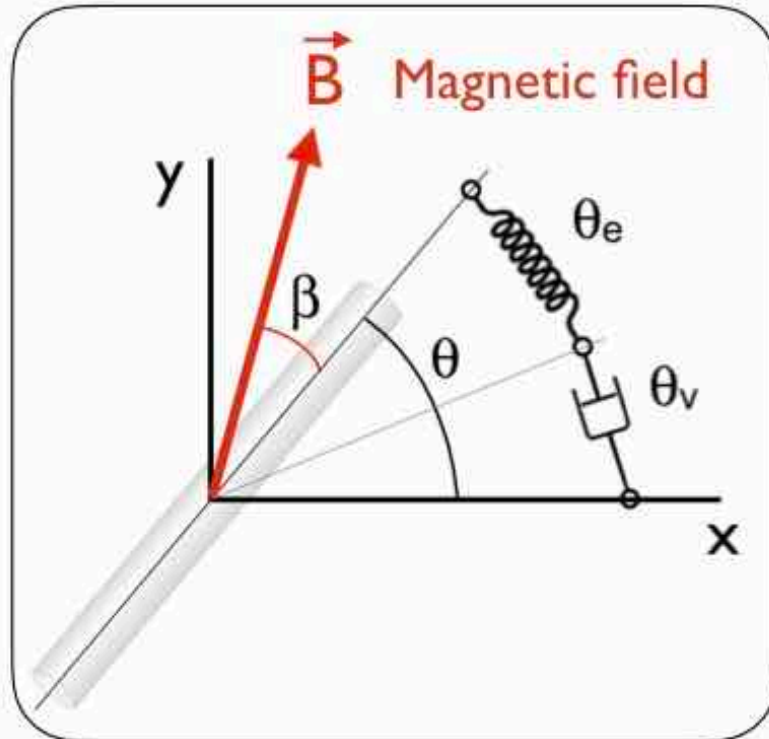
Standard Linear Solid model



→ Soft Solids

The rotation behavior depends on the rheological properties of the fluid/material surrounding the wire

Maxwell model



- Differential equation

$$\frac{d\theta(t)}{dt} = \frac{\omega_c \sin 2(\omega t - \theta) + \omega \theta_0 \cos 2(\omega t - \theta)}{(1 + \theta_0 \cos 2(\omega t - \theta))}$$

↖ Elastic modulus
↘ Viscosity

$$\longrightarrow \theta(t, \omega)$$

Analogy with classical rheology using stress, strain and shear rate

- Magnetic torque

$$\Gamma_{Mag}(B) = \frac{\Delta\chi V}{2\mu_0} B^2 \sin 2(\omega t - \theta)$$

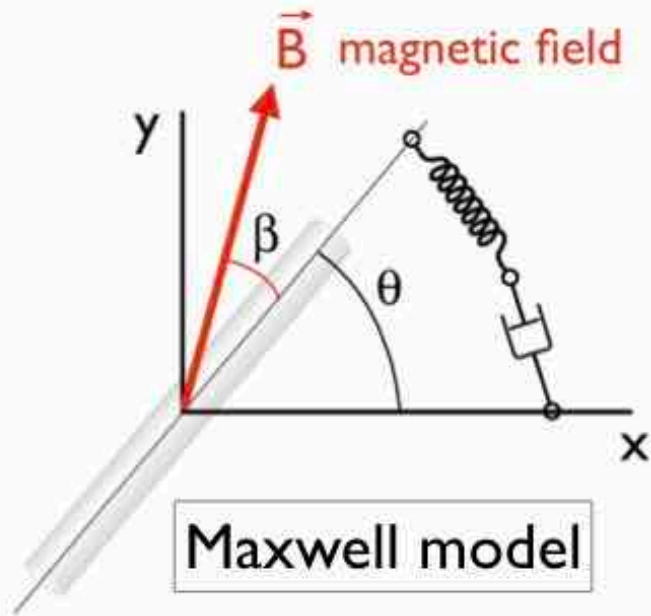
- Viscous torque

$$\Gamma_{Vis} = \frac{\pi \eta L^3}{3g(L/D)} \frac{d\theta_v}{dt}$$

- Elastic torque

$$\Gamma_{El} = \frac{\pi G L^3}{3g(L/D)} \theta_{El}$$

L wire length
D wire diameter
η static viscosity
G elastic modulus



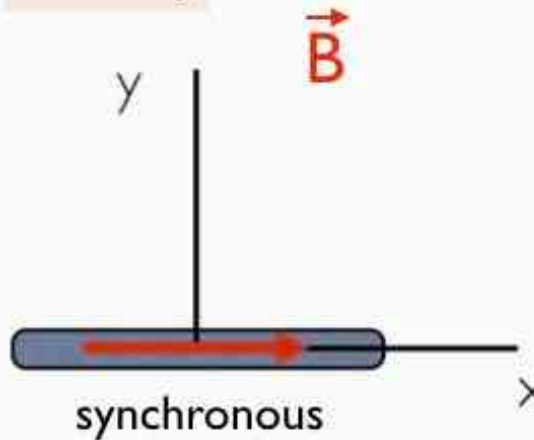
$$\omega_c = \frac{3 \Delta\chi B^2}{8\mu_0 \eta L^2}$$

$$\lim_{\omega \rightarrow \infty} \theta_B = \theta_0 = \frac{3 \Delta\chi B^2}{4\mu_0 G L^2}$$

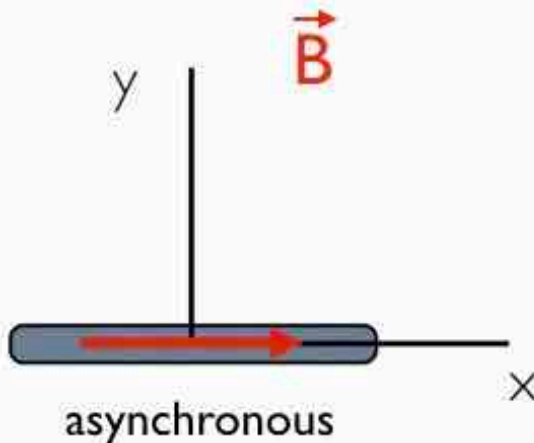
L wire length
D wire diameter
 η static viscosity

H magnetic field
 $\Delta\chi$ susceptibility anisotropy

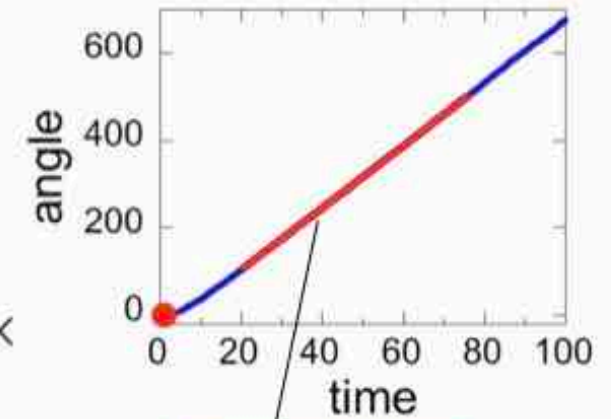
$\omega \leq \omega_c$



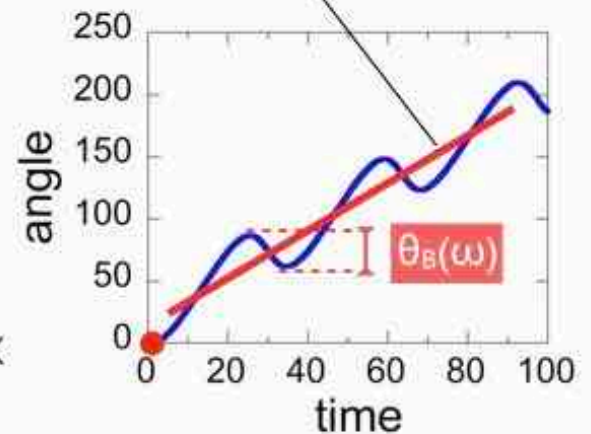
$\omega > \omega_c$



$\theta(t, \omega)$

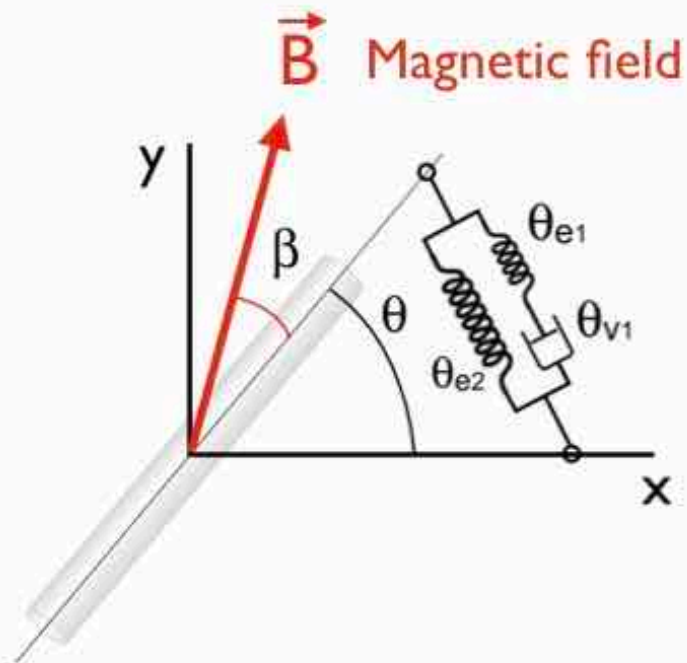


$\Omega(\omega)$ average rotation velocity



Predictions

- Yield stress materials
- Concentrated colloids
- Gels



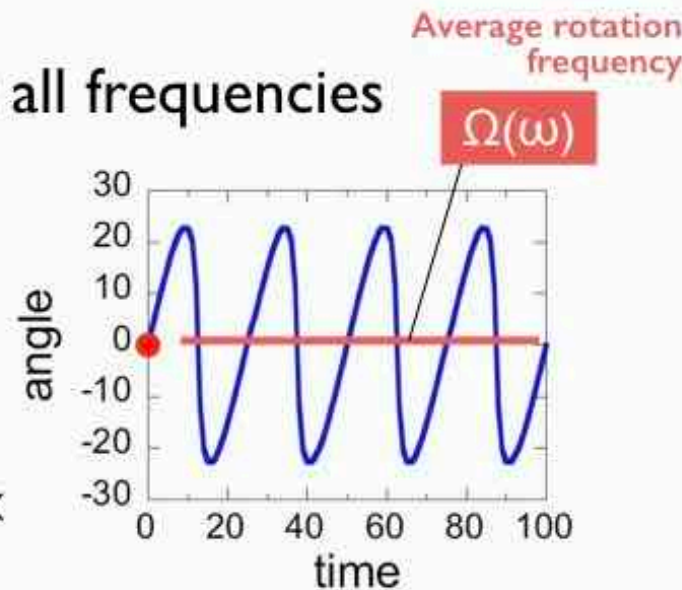
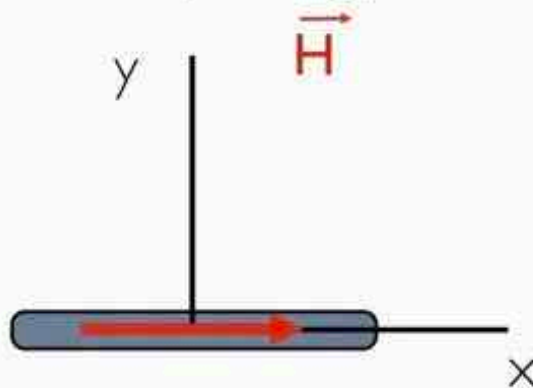
Standard Linear Solid model

$$\omega_c = \frac{3}{8\mu_0} \frac{\Delta\chi B^2}{\eta L^{*2}} = 0$$

$$\lim_{\omega \rightarrow 0} \theta_B(\omega) = \frac{3}{4\mu_0} \frac{\Delta\chi B^2}{G_{eq} L^{*2}}$$

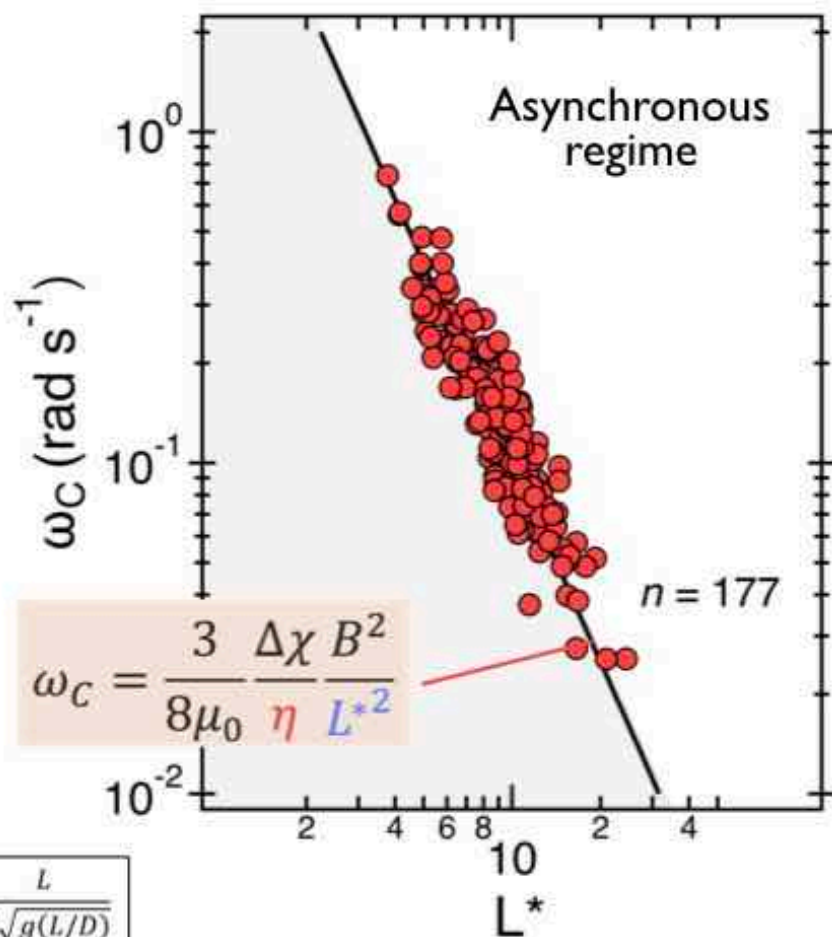
L wire length
D wire diameter
 η static viscosity
G elastic modulus

→ a unique regime at all frequencies

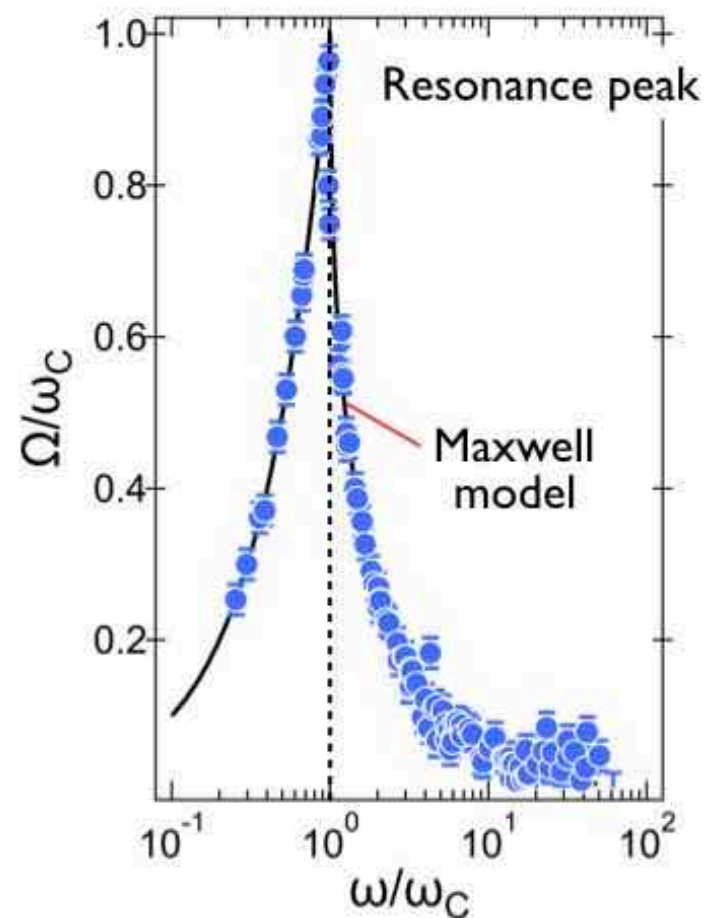


MRS differentiates viscoelastic liquid from soft solids

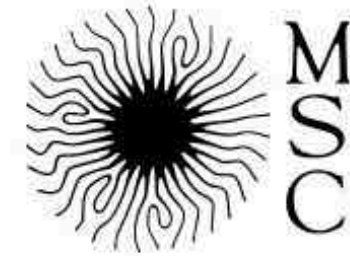
Water-Glycerol



Wormlike micelles



Accessible ranges: Viscosity 0.001 - 1000 Pa s - Elastic modulus 0.01 - 100 Pa



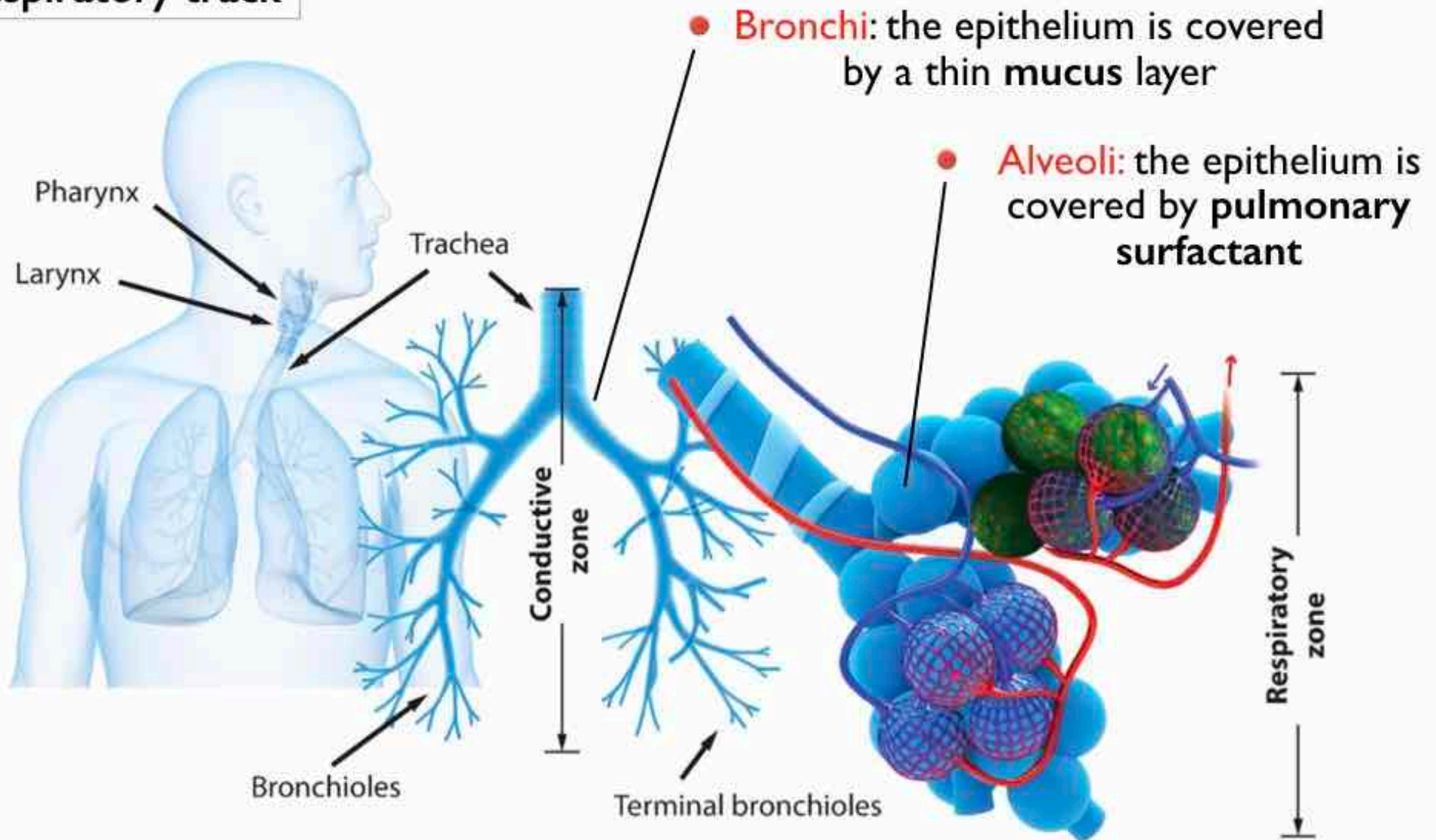
Matière et Systèmes Complexes

I - The tools

II - Rheological models and validation

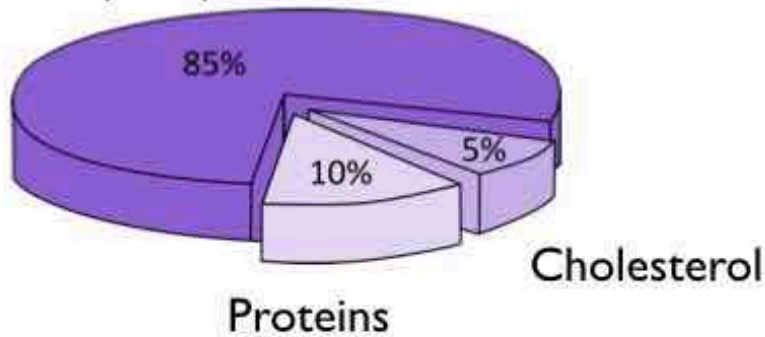
III - Applications to lung fluids

Respiratory track



Composition

Phospholipids



lipid/protein conc. : 40 g L⁻¹

Specific proteins

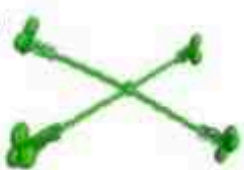
SP-A



SP-B



SP-D



SP-C

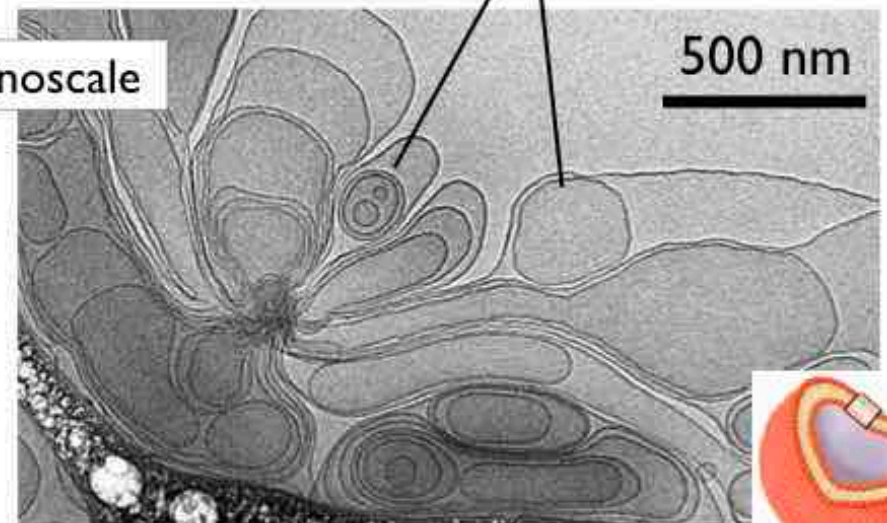


Curosurf®



- From Chiesi (Italy)
- Porcine origin
- Administered to premature infants (< 32 weeks)
- **Multivesicular vesicles** (negatively charged)

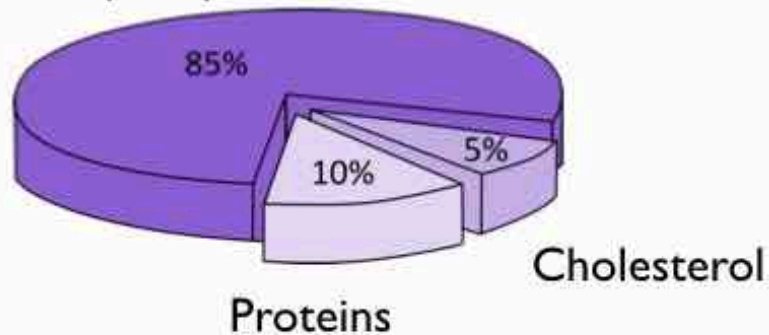
Nanoscale



Phospholipid vesicle

Composition

Phospholipids



lipid/protein conc. : 40 g L⁻¹

Specific proteins

SP-A



SP-B



SP-D



SP-C

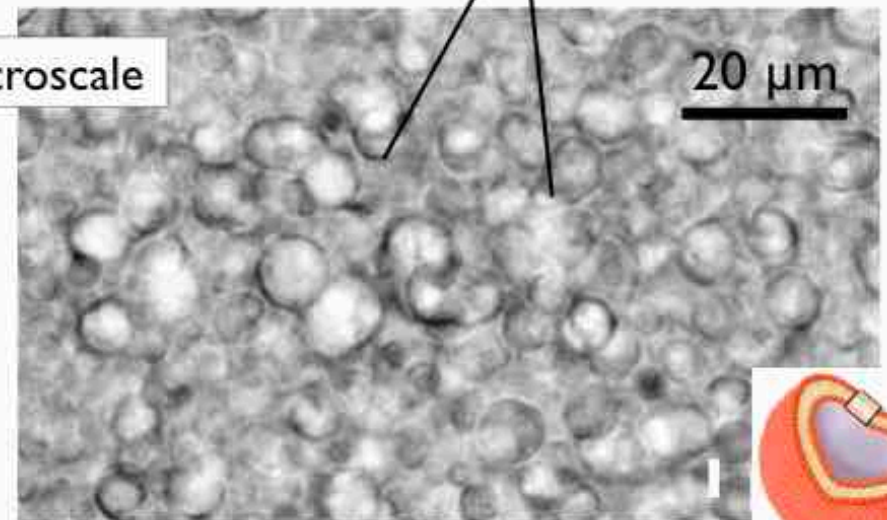


Curosurf®



- From Chiesi (Italy)
- Porcine origin
- Administered to premature infants (< 32 weeks)
- **Multivesicular vesicles** (negatively charged)

Microscale



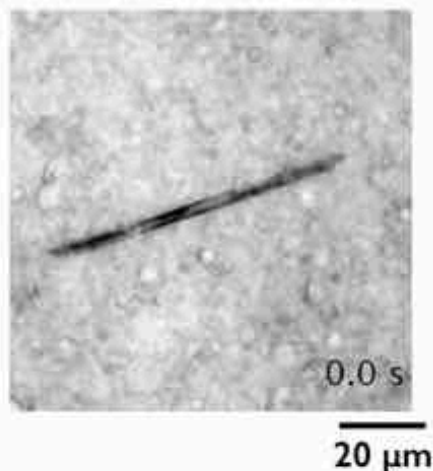
Phospholipid vesicle



Krieger-Dougherty

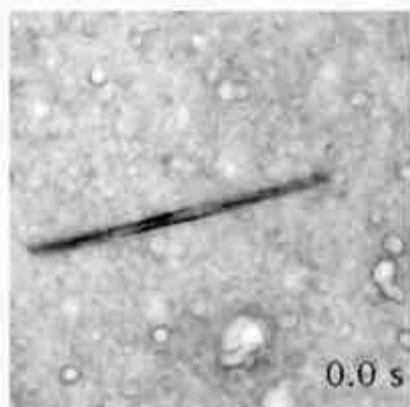
$$\eta_{K-D}(c) = \eta_s \left(1 - \frac{c}{c_m}\right)^{-2}$$

Synchronous rotation



ω_c

Hindered rotation

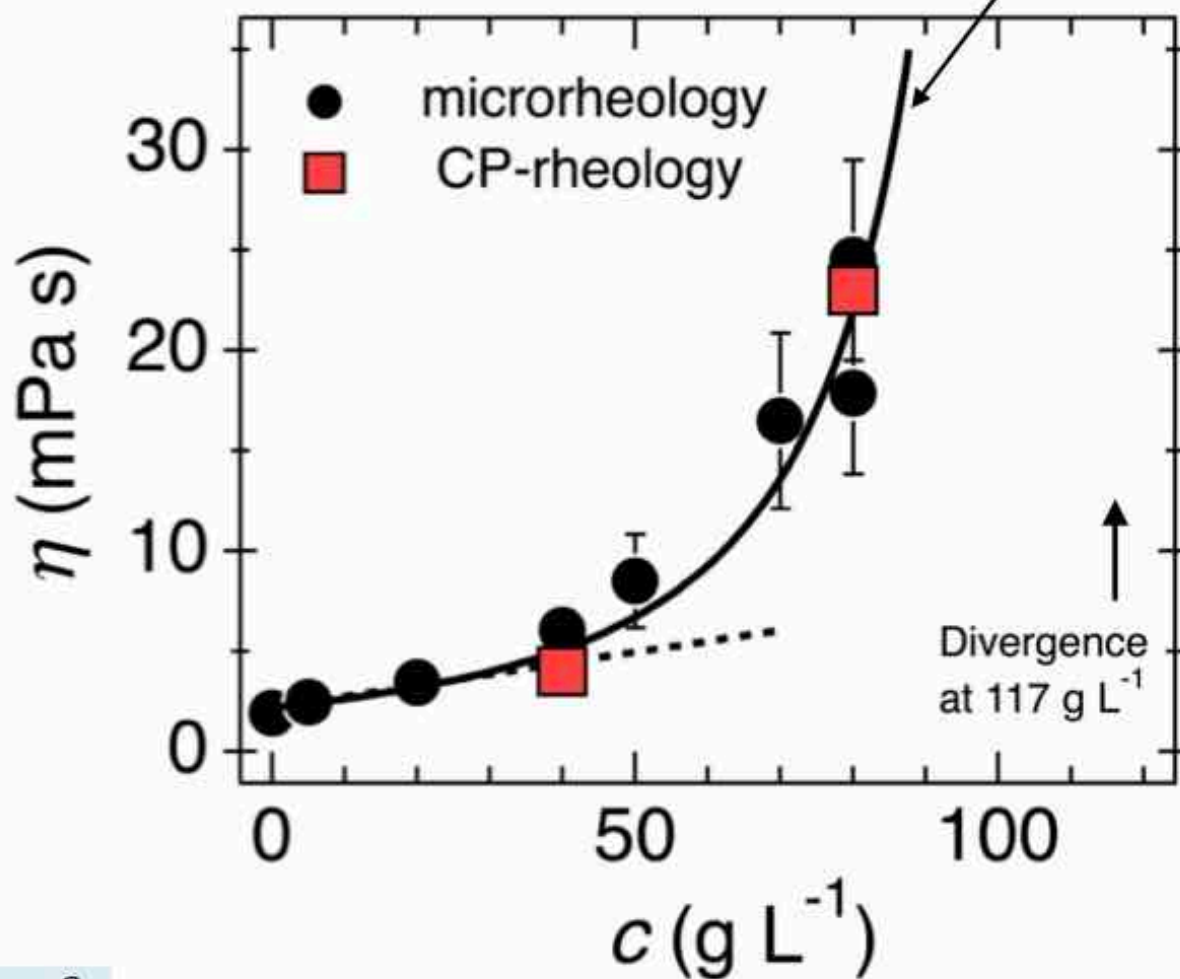


frequency

$$\omega_c = \frac{3}{8} \frac{\mu_0 \Delta\chi}{\eta} \frac{H^2}{L^2}$$

L wire length
D wire diameter
 η static viscosity

H magnetic field
 $\Delta\chi$ susceptibility anisotropy



Divergence at 117 g L⁻¹



Pulmonary mucus

Healthy versus inflamed bronchus

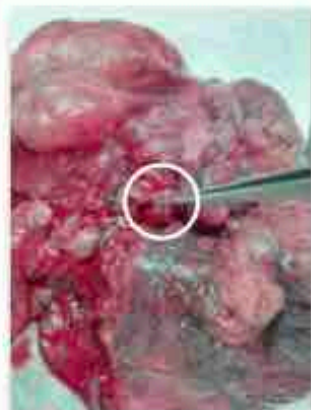


Pr. Xavier Norel
Bichat Hospital (UPC)

Human lungs from the anatomical pathology department at Bichat Hospital



Excised lung



Bronchial tube

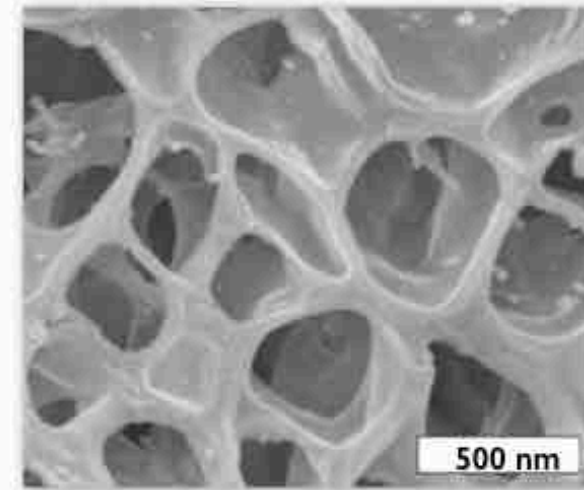
In vitro
mucus



In vivo
mucus



Mucus is a porous viscoelastic gel made from mucin proteins



Highlights

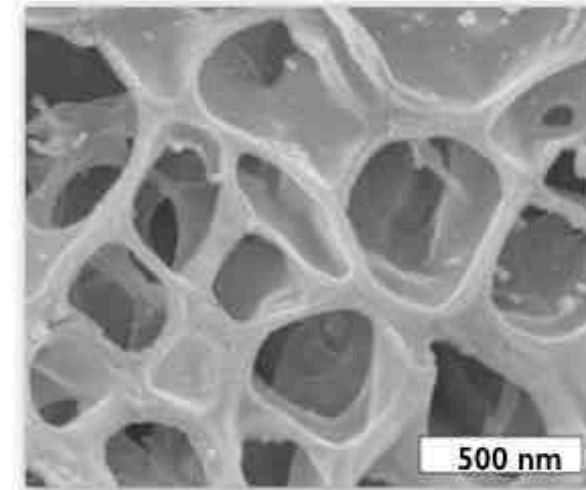
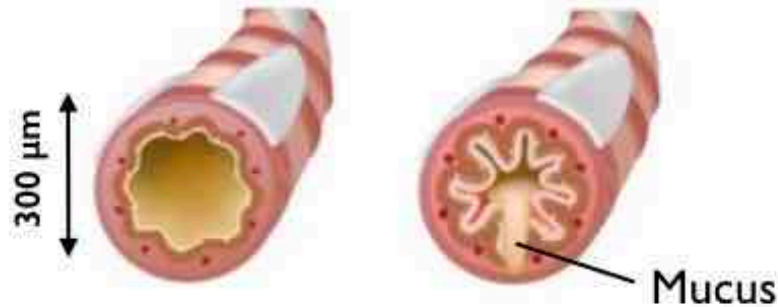
- First determination of simultaneous viscosity and elasticity on human pulmonary mucus
- Mucus is a weak viscoelastic liquid with low elasticity (few Pa) and very high viscosity (few 100 Pa s)



Pulmonary mucus

Mucus is a porous viscoelastic gel made from mucin proteins

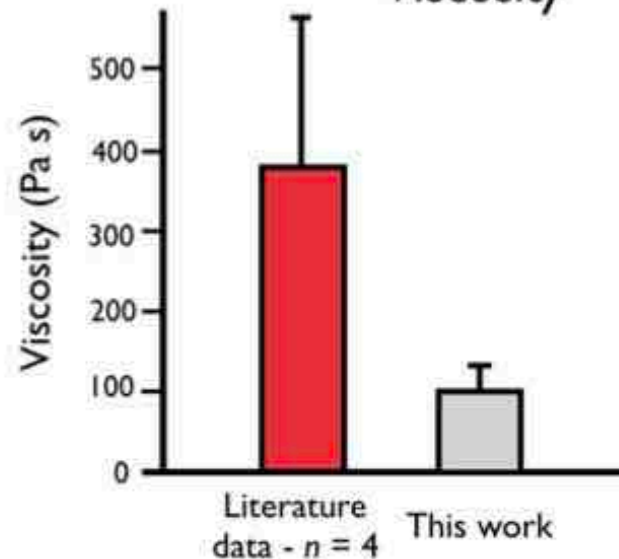
Healthy versus inflamed bronchus



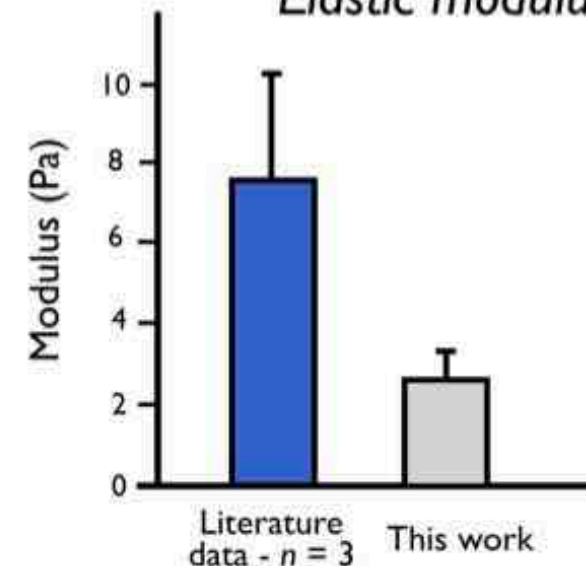
Pr. Xavier Norel
Bichat Hospital (UPC)

Highlights

Viscosity



Elastic modulus



- Magnetic Rotational Spectrometry (MRS) is simple and quantitative
- It measures the rheological properties of complex fluids and materials in the ranges

Frequency 10^{-4} - 100 Hz
 Viscosity 0.001 - 1000 Pa s
 Elastic modulus 0.01 - 100 Pa

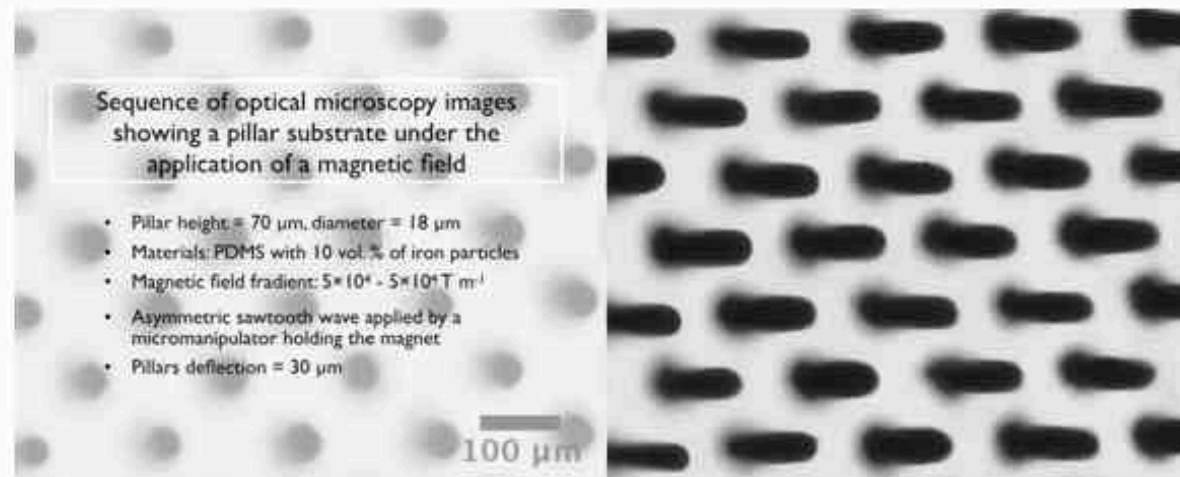
- MRS has been applied to wormlike micelles, polysaccharide gels, live mammalian cells, lung fluids and bacterial amyloids
- MRS is doomed to become a classical tool for easy-to-use microrheology





24-month POST-DOCTORAL FELLOWSHIP

Lab-on-a-chip model of mucociliary clearance for the treatment of Inflammatory Lung Diseases



Interested? Please contact me at jean-francois.berret@u-paris.fr

University Paris-Cité

Xavier Norel

Véronique Arluison

Fanny Mousseau

Milad Radiom

Evokia K. Oikonomou

Aline Grein Iankovski

Rémi Le Borgne

Foad Gahsemi

Le-Phuong-Anh Thai

Sorbonne Université

Jérôme Fresnais

University Bordeaux

Olivier Sandre

Solvay

Annie Vacher

Marc Airiau

University of Riga Latvia

Andrejs Cebers

Universidad Complutense de Madrid

Fernando Martínez-Pedrero

Thank you for your attention

The lecture can be found at:

<https://www.jean-francois-berret-website-pro.fr>